#### A FINITE ELEMENT MODEL FOR DETERMINING THE EFFECTS OF BLOOD FLOW ON THE FINGER TEMPERATURE DISTRIBUTION

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#### **The Physiological Characteristics of the Human Finger**

- The vessel network is well developed
- Compared to the other parts in human body, there are fewer muscles
- When human body receives an inside and outside stimulus, the physiological behavior in the hand will vary obviously.

### **The Mechanical Characteristics of the Human Finger**

- The human finger has high sensory and motor capacities
- Convey information about (a) mechanical, (b) thermal and (c) tissue damaging events occurring on the skin of the hand

#### Some Physiological Phenomena and Diseases Related to Finger Skin Temperature

• After cigarette smoking, the peripheral circulation becomes worse and the skin temperature decreases. (Cleophas,T.J.M, et al. 1982, Bornmyr, S. et al. 1991)

- While in the state of stress or fatigue, the finger skin temperature decreases (Nketia,P. and Reisman,S. 1997).
- Thermoregulation abilities for men and women are different (Cooke,J.P. et al. 1990)
- Raynaud's syndrome

#### **Research Objective**

• What is the mechanism of thermoregulation and circulation diseases in periphery.

• Numerous thermal models have been presented, few models focused on the relationship between haemodynamic changes and heat transfer.

#### The possible applications

Developing human sensory sensor used in the areas like:

- Health management for monitoring physiological parameters
- Safe driving
- Family robot and prosthetic hands



## The peripheral circulation system in the hand (cited from Angiology and Taschenatlas der Anatomie)



1. Bone 2. Tendon 3. Dermis 4. Epidermis 5. Artery

Two-dimensional thermal model of the middle finger

#### The geometric model of the finger in longitudinal direction



Blood flow:

Laminar flow

Blood vessels:

rigid tube, the tube elasticity is not considered.

#### Governing Equations in Blood Vessels

• Navier-Stokes equation

$$\frac{\partial \mathbf{u}}{\partial t} + (\mathbf{u} \cdot \nabla)\mathbf{u} = -\nabla p + \frac{1}{\mathrm{Re}} \mathbf{u}$$

• Continuity equation

 $\nabla \cdot \mathbf{u} = 0$ 

• Energy equation

$$\frac{\partial \mathbf{T}}{\partial t} + (\mathbf{u} \cdot \nabla) = \frac{1}{Pe} \quad T$$

u:	velocity
p:	pressure
T:	temperature
Re:	Reynolds number
Pe:	Peclet number

#### Energy Equation in tissues

$$\frac{\partial \mathbf{T}}{\partial t} = \frac{1}{Pe_t} \quad \mathbf{T} + \frac{\psi}{Pe_b} W(1 - \mathbf{T}) + \frac{\psi}{Pe_b} q_{met}$$

u:velocityT:temperature $T = \frac{T^* - T_{\infty}^*}{T_a^* - T_{\infty}^*}$ Pe:Peclet number $Pe_t = \frac{U_{\infty}D}{\alpha_t}$ W:dimensionless volumetric blood perfusion rate $W = \frac{(\omega_b \rho_b c_b)D^2}{\lambda_b}$  $\psi$ :dimensionless ratio of blood to tissue thermal inertia $\psi = \frac{\rho_b c_b}{\lambda_b}$  $q_{met:}$ dimensionless volumetric heat generation rate $q_{met} = \frac{q_{met}^*D^2}{(T_a^* - T_{\infty}^*)\lambda_b}$ subscriptst:tissue

b: blood



#### **Characteristics and limitations**

- The Governing equations of fluid are suitable for the whole domain (fluid and solid part)
- No necessary to consider the boundary conditions between fluid and solid part
- Can deal with the problem with different thermal properties in different place
- Be applicable to the thermo-fluid problem in low Reynolds number
- not easy for mesh generation
- The computational time is increased

#### **Boundary conditions**

- 1. Inlet part: *u*=1, *v*=0, *T*=1
- 2. Outlet part: p=p<sub>out</sub>
- 3 . Solid tissue (inside): u = v = 0
- 4. Cross section (solid): u=v=0

$$T = T_1(y,t) \text{ or } T = T_1(y)$$

- 5. Skin surface: Temperature
  - *a*. In the air:
- Bi: Biot number

$$\begin{aligned} u = v = 0\\ \frac{\partial T}{\partial n}\Big|_{\Gamma} = BiT\Big|_{\Gamma} + \frac{h_{ra}D}{\lambda_s}\Big| + E_{diff}\end{aligned}$$

# Table 1. Thermophysical properties and bloodperfusion rate of tissues

	bone	tendon	skin	blood
$\rho(kg/m^3)$	1418	1270	1200	1100
c(J/kgK)	2094	3768	3391	3300
$\lambda(W/mK)$	2.21	0.35	0.37	0.50
$\omega$ (ml/ml/min)	2.0/100	3.43/100	24/100	_
$\mu \times 10^{6} (N.s/m^{2})$	_	_	_	2085
$q_{met}(W/m^3)$	352	368	273	_

Arterial temperature	37°C
Outlet pressure	20 mmHg
Ambient temperature	19°C
(by infra-red thermography)	
Arterial blood velocity (by	6, 10, 20cm/s
bi-directional Doppler	
DVM-4300)	
Convective heat transfer	4W/m <sup>2</sup> K
coefficient	
Radiative heat transfer coefficient	$ 4.7W/m^2K $

A part of finite element grid network of the modeled finger in longitudinal direction



elements: 19234

time increment:

2 × 10<sup>-5</sup>

 $2 \times 10^{-3}$ (only in the energy equation)



a. Velocity distribution b. Isotherm contours of model-A finger in longitudinal direction for different blood velocity



Temperature profile in a cross section of a finger for different blood flow conditions



a. The comparison of the measured skin temperature and the computed skin temperature b. The thermograph of a finger (ambient temperature  $T_{amb}=19^{\circ}C$ )

#### Isotherm contour and temperature profile of model-B finger







#### **Concluding Remarks**

• A FE thermo-fluid model is presented to investigate the effect of blood flow on the temperature distribution in a finger.

• In indoor environment, with the velocity in larger blood vessels increasing, the skin temperature increases. However, the variations of the skin temperatures in different blood velocities are quite small .

• The comparison of the results of model A and B suggest that the heat transport in the superficial vein is important.

#### Discussion

- The flexibility of the blood vessel, the waveform velocity, and the transmural pressure may be considered in examining the relationship between the flow rate and temperature in the peripheral circulation.
- In order to simulate the thermal characteristic of human body in the dynamic state, the coupling of one-dimensional elastic model and FE thermal model is expected.